

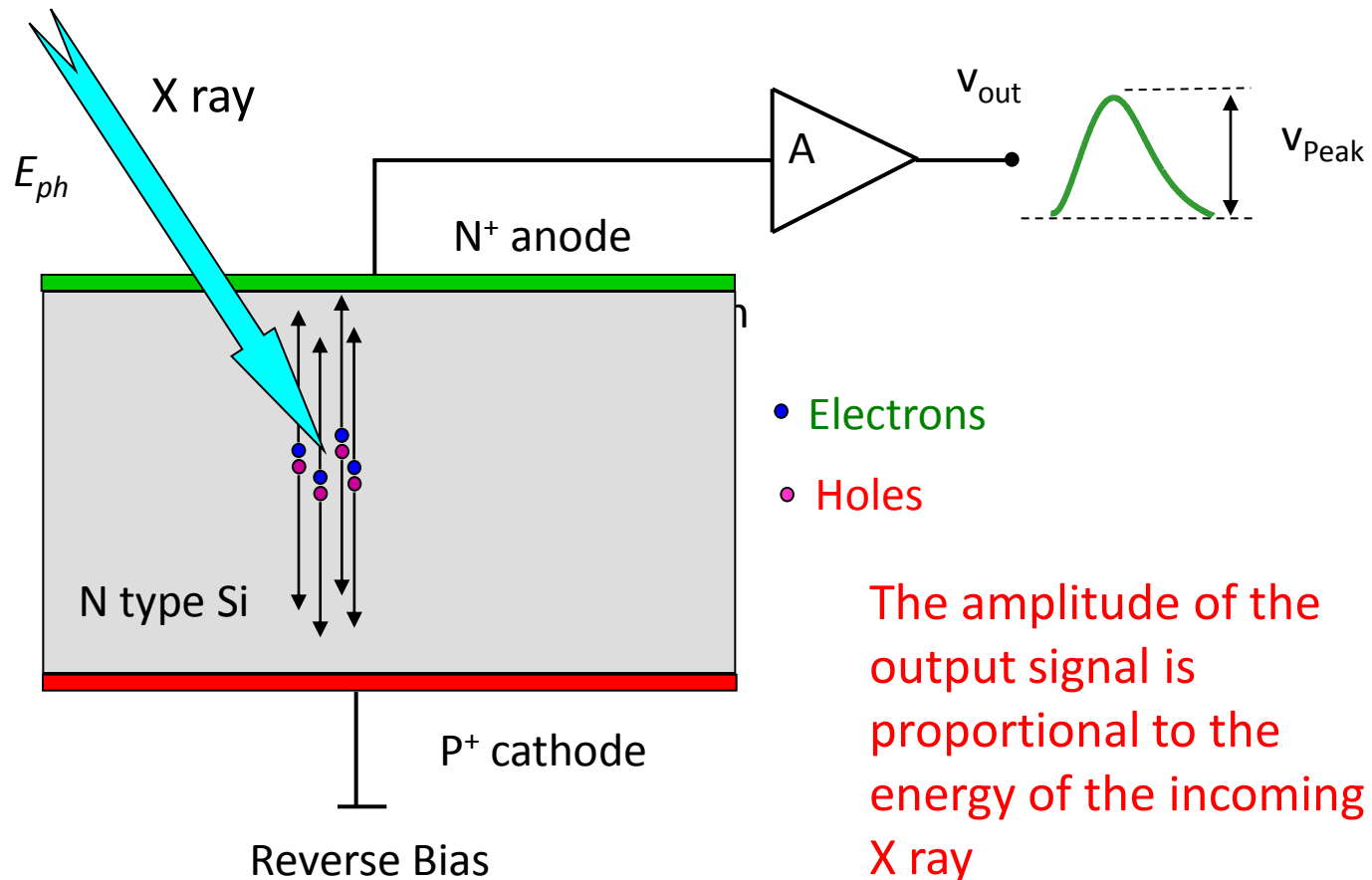
Silicon Drift Detectors for gamma-ray detection:
15 years of research
(and collaboration between Politecnico and INAF-Milano)

Outline

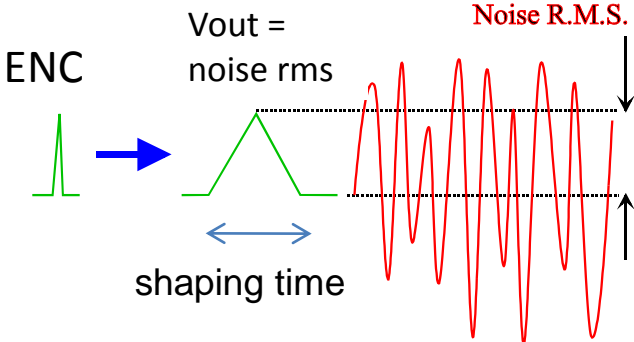
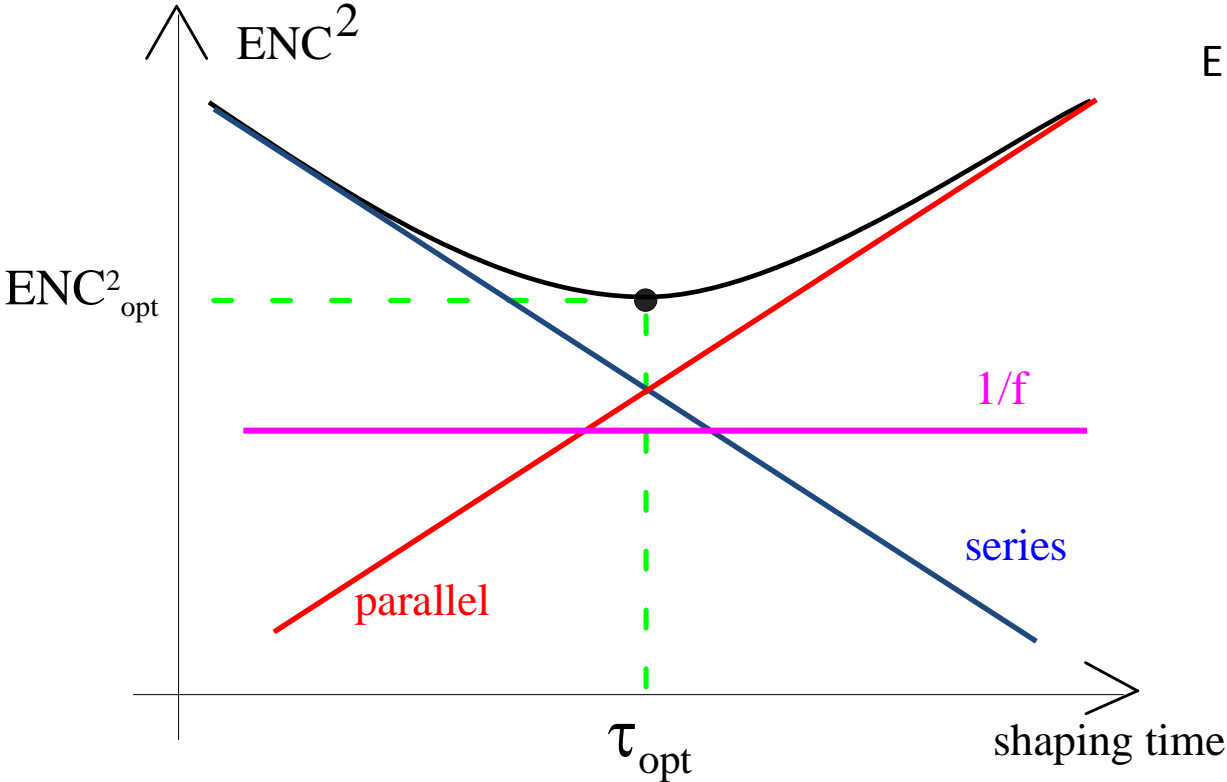
- The Silicon Drift Detector (SDD)
- Gamma-ray detectors based on scintillators and SDDs
- Applications
- Future activities



X-ray interaction in a semiconductor detector, generation of the output signal



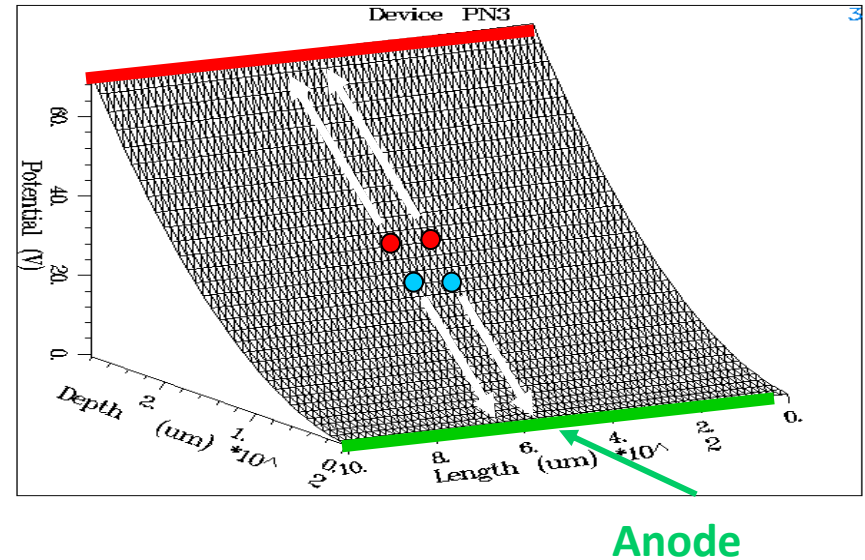
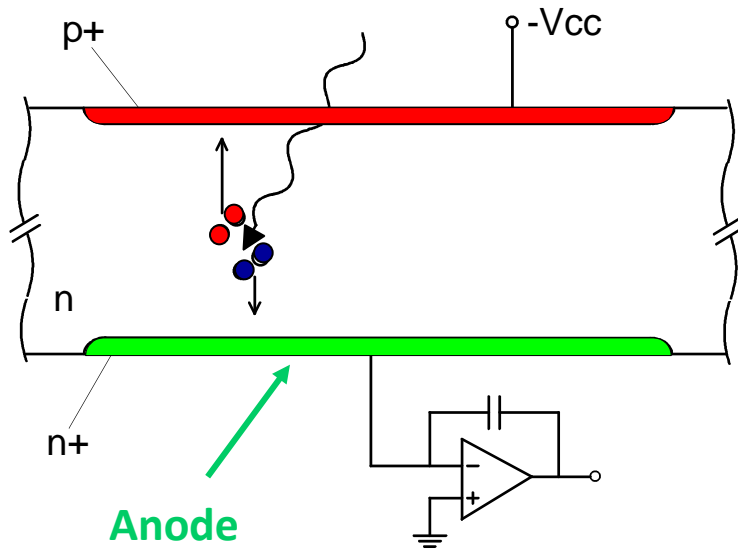
Equivalent Noise Charge (ENC)



$$ENC^2 = A_1 \underbrace{2KT\alpha}_{\text{series}} \underbrace{1/gm}_{\text{series}} \underbrace{(C_D + C_i)^2}_{\text{series}} \underbrace{\frac{1}{\tau}}_{\text{series}} + A_2 q \underbrace{I_{leak}}_{\text{parallel}} \tau + A_3 \underbrace{2\pi A_F}_{\text{1/f}} \underbrace{(C_D + C_i)^2}_{\text{1/f}}$$



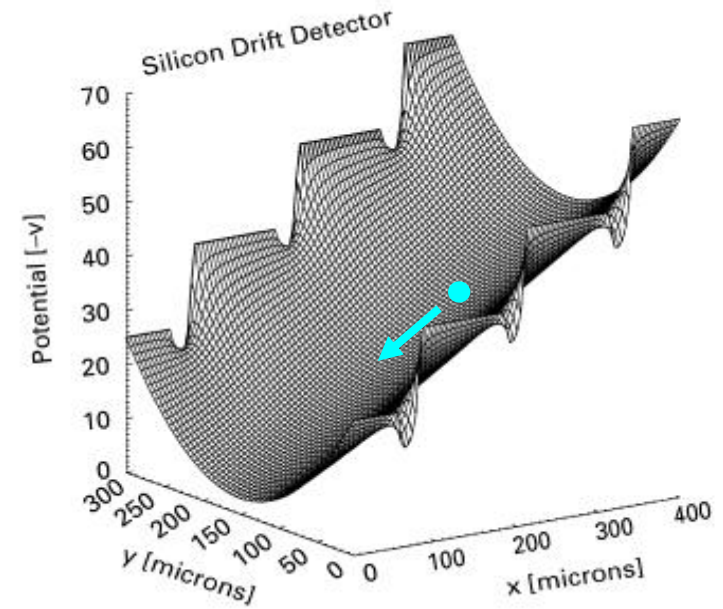
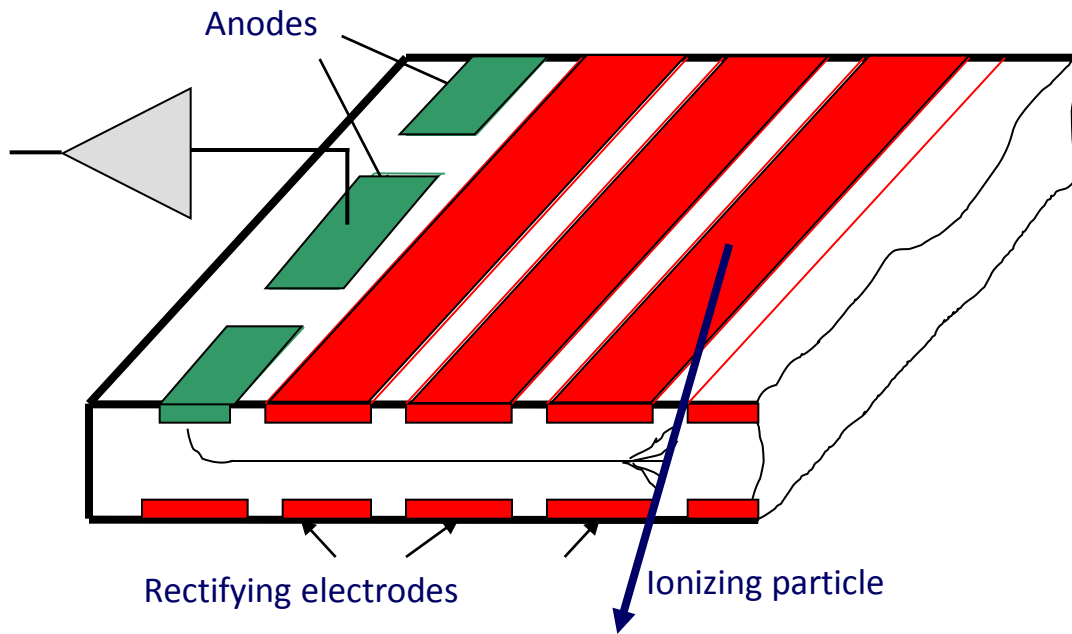
The classical PIN diode detector



- The diode is reversely biased in order to fully deplete from free carriers the semiconductor bulk.
- The electrons generated by the X-ray interaction are collected at the anode, the holes at the cathode.

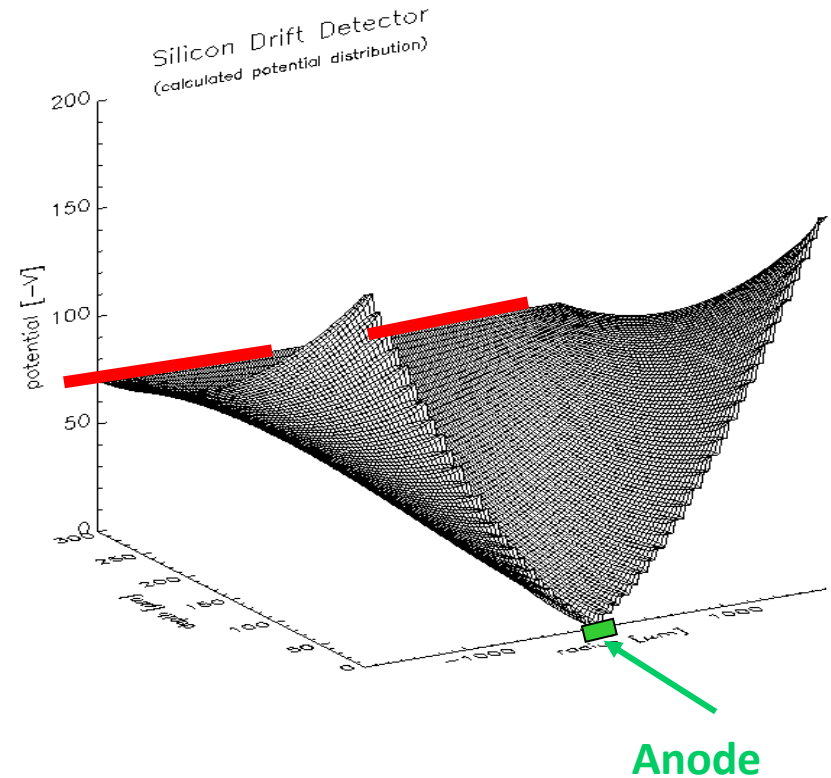
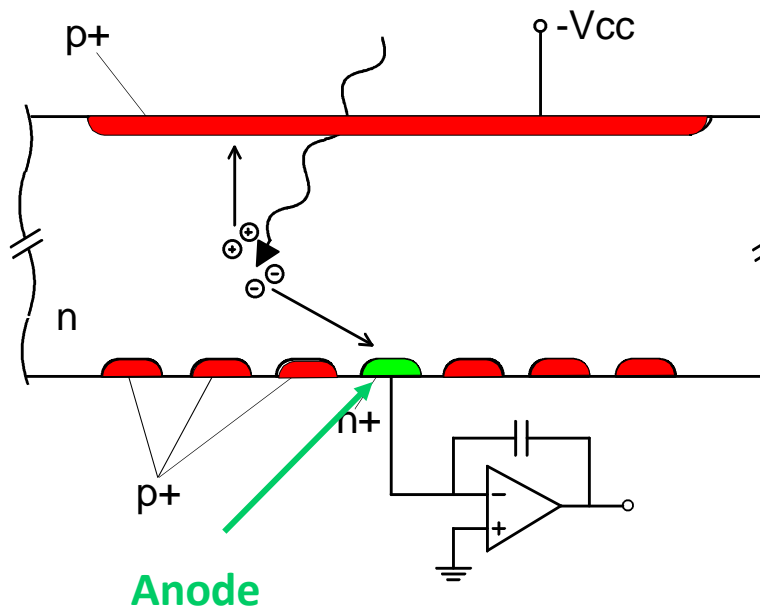
The detector capacitance C_D is proportional to the active area

The Silicon Drift Detector (SDD)



The concept of the SDD has been introduced by E.Gatti (Politecnico di Milano) and P.Rehak (Brookhaven National Laboratory) in 1983

The SDD for X-ray spectroscopy



The electrons are collected by the small anode, characterised by a **low output capacitance**, whose value is independent on the active area of the detector.

Observed energy dependence of Fano factor in silicon at hard X-ray energies

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Received 29 July 1998; received in revised form 15 September 1998

N_e : numero di elettroni generati da un evento ionizzante

$N_e = E/\varepsilon$ con E =energia, $\varepsilon = 3.6\text{eV}$ in Silicio

$\sigma_{N_e}^2$: varianza

$$\sigma_{N_e}^2 = N_e \cdot F$$

F : fattore di Fano (ca. 0.12 in Si)



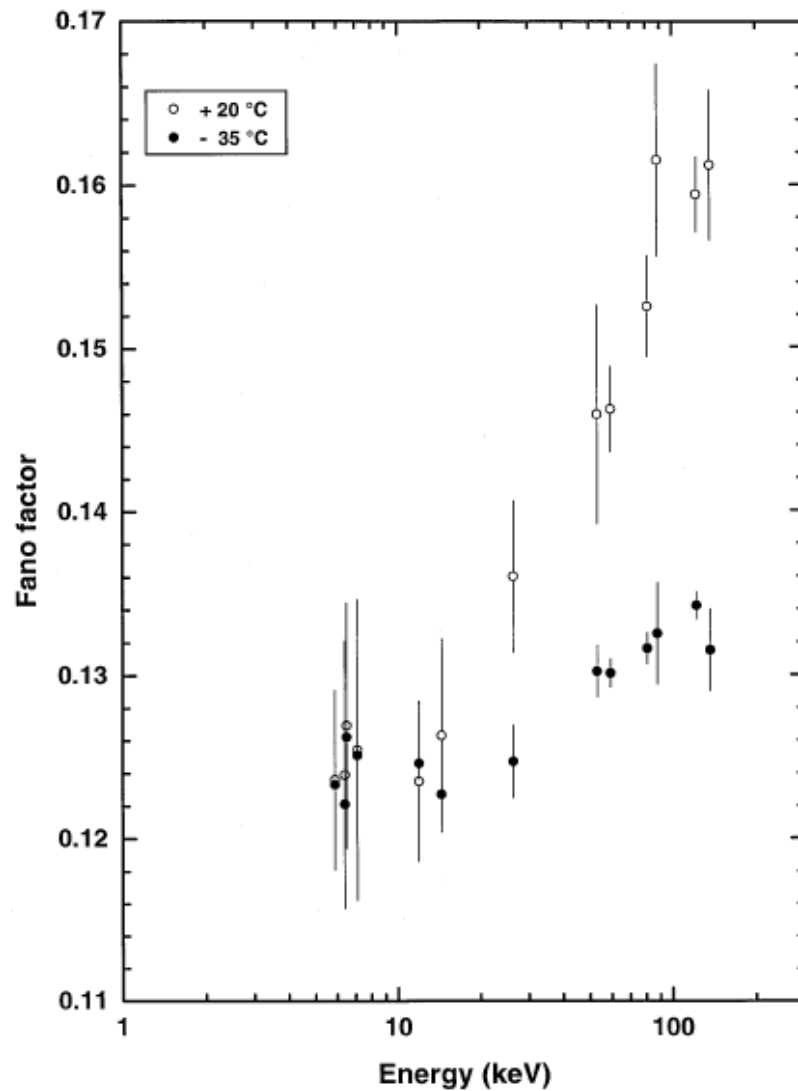
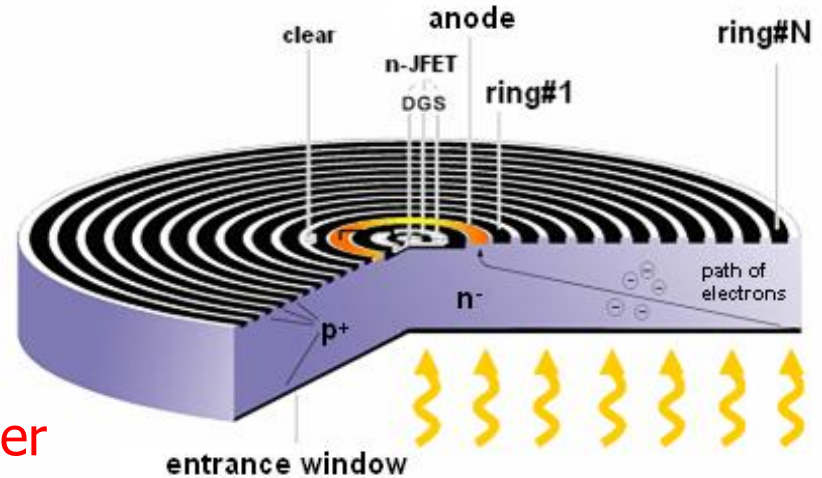
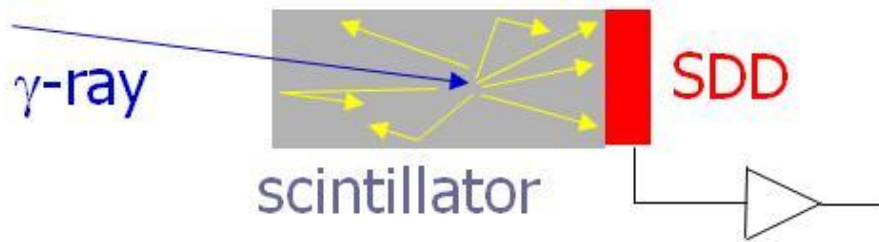


Fig. 7. Fano factor evaluated at room temperature and at -35°C as a function of the energy of the X-ray detected photons.

Application of the SDD in γ -ray spectroscopy and imaging



Advantages of SDDs with respect to other photodetectors:

- high quantum efficiency ($\sim 90\%$) @ 565nm of CsI(Tl), vs. PMT($\sim 30\%$ of PMT)
- compact, mechanical robust
- no statistical spread due to multiplication
- low operating voltages
- smaller sensitivity to bias and temperature variations
- insensitivity to magnetic fields

Applications:

- medical imaging
- gamma-ray astronomy
- homeland security
- nuclear physics experiments

Scintillation detection using a silicon drift chamber with on-chip electronics

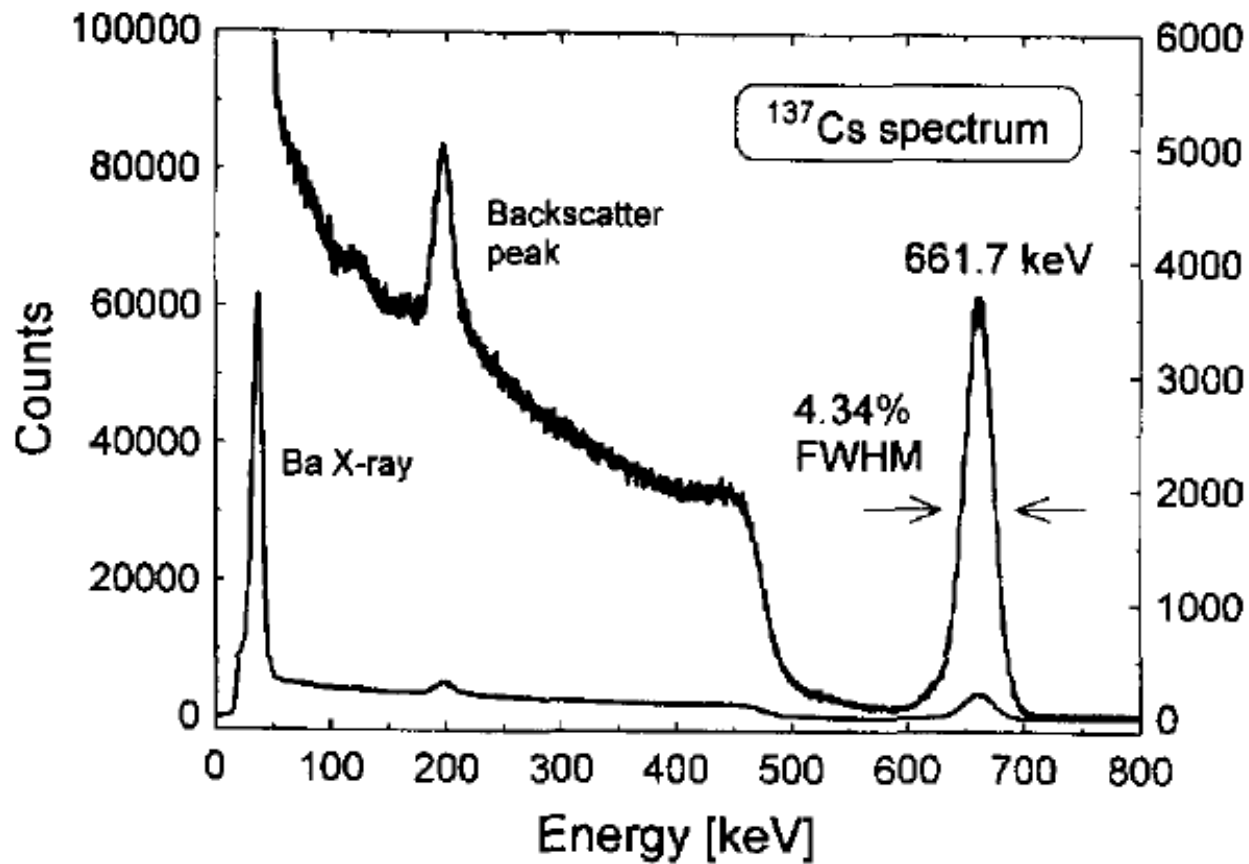
C. Fiorini^{a,*}, F. Perotti^b

^a *Politecnico di Milano, Dipartimento di Elettronica e Informazione, Piazza L. da Vinci 32, 20133 Milano, Italy*

^b *Istituto di Fisica Cosmica e Tecnologie Relative, C.N.R., via Bassini 15, 20133 Milano, Italy*

Received 16 June 1997





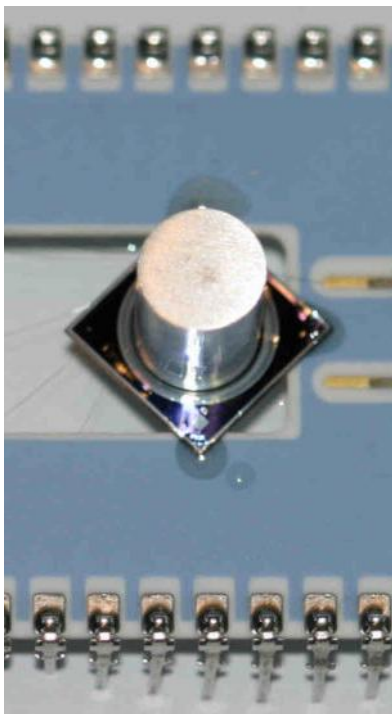
Gamma-ray spectroscopy with a SDD coupled to a CsI(Tl) scintillator

at the time of publication, the world-record energy resolution with a scintillator

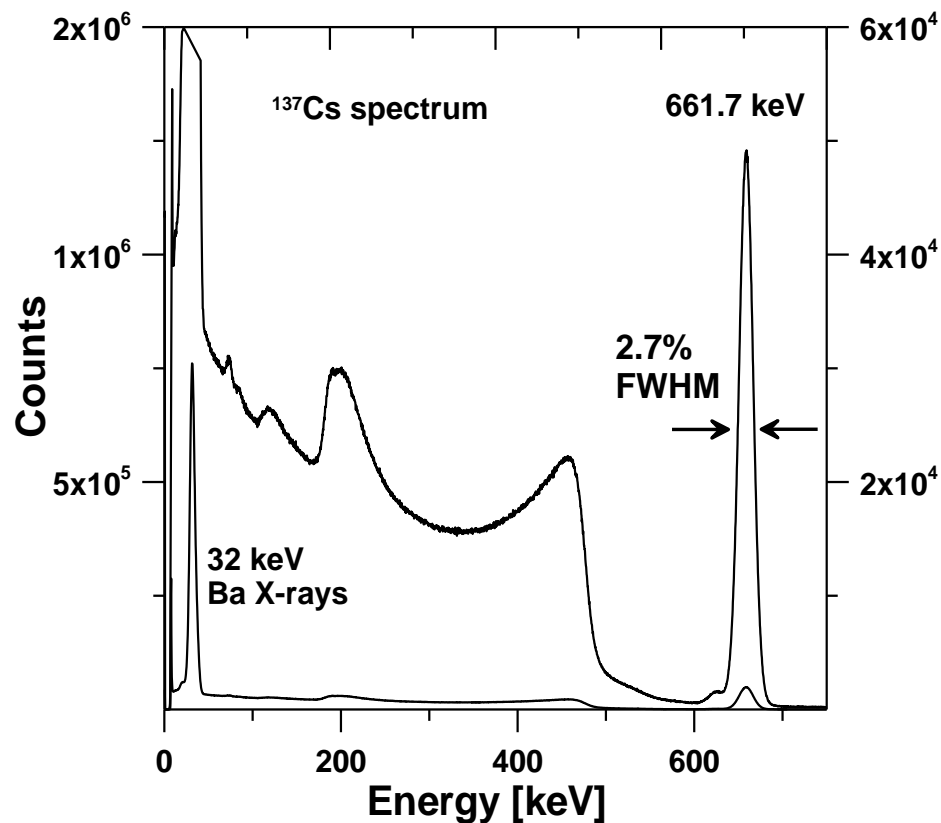
Measurement carried out at CNR – Via Bassini – the 31 December 1996



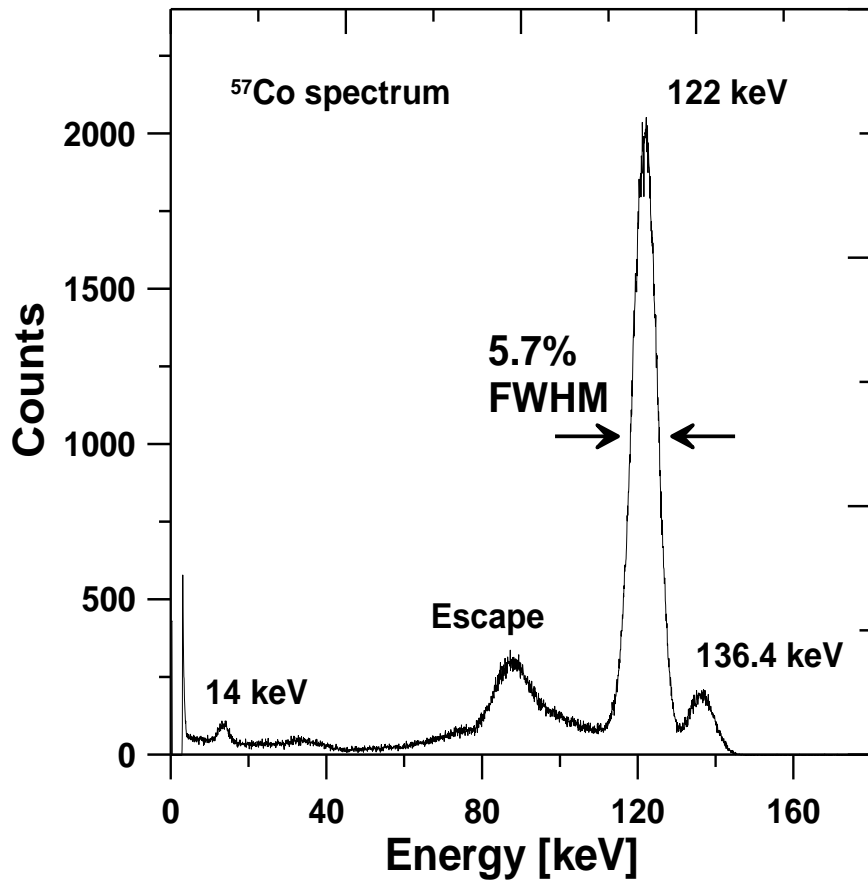
Gamma-ray spectroscopy with an SDD coupled to LaBr₃



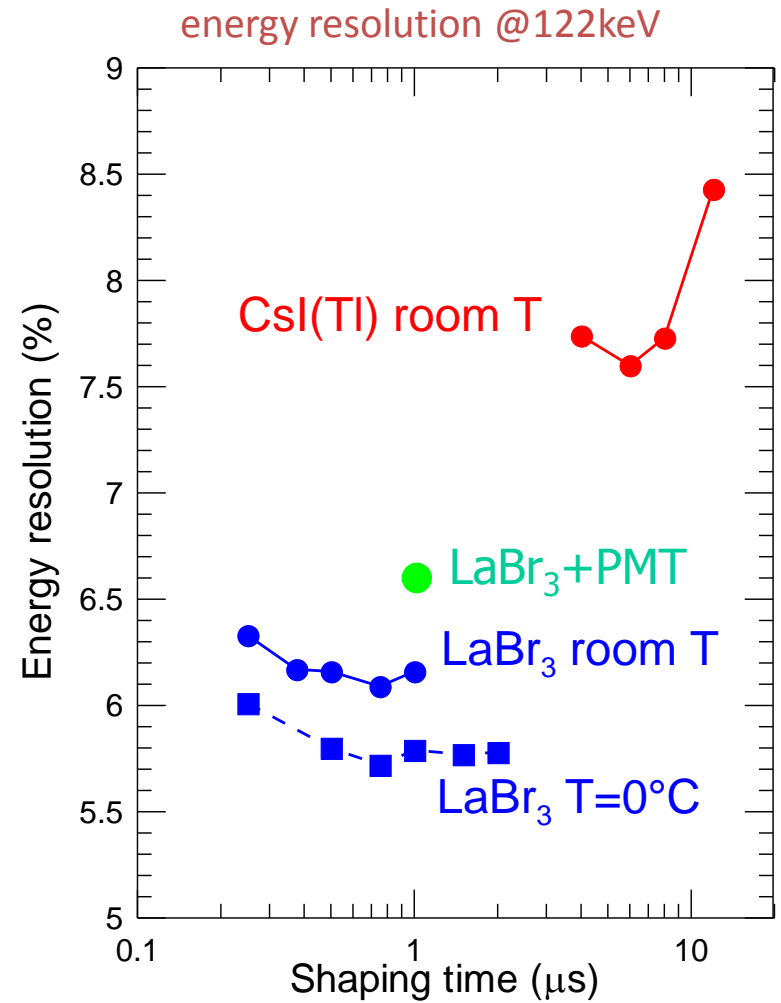
- 30mm² SDD
- Brilliance 380
5mm Ø,
5mm thick



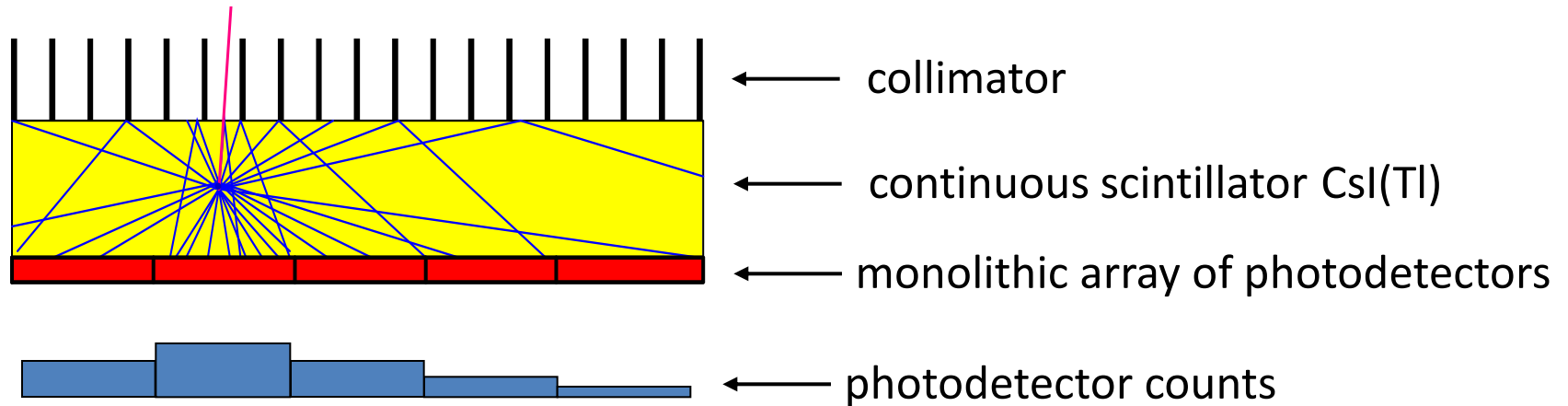
Fiorini, C.; et al. "Gamma-Ray Spectroscopy With LaBr₃:Ce Scintillator Readout by a Silicon Drift Detector"; IEEE Transactions on Nuclear Science, Volume 53, Issue 4, Part 2, Aug. 2006 Page(s):2392 – 2397.



world record in energy resolution with a scintillator



Anger Cameras based on SDDs



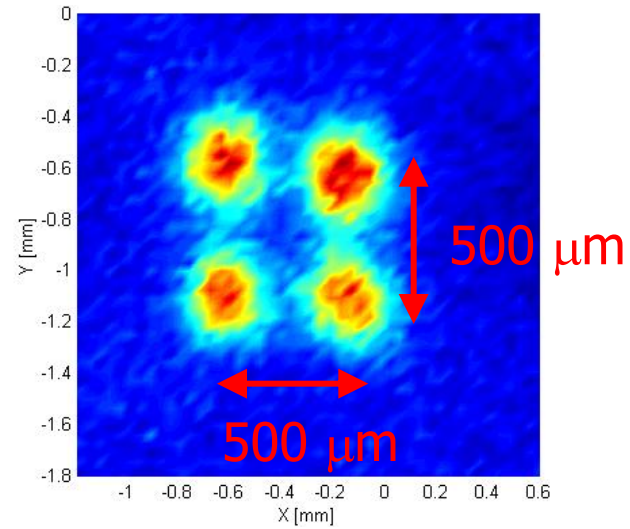
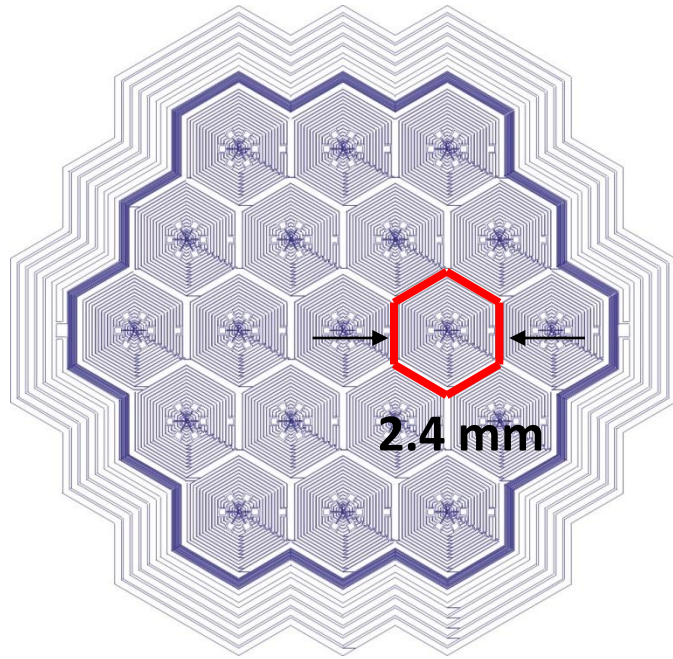
Main advantages (vs. pixellated detectors, e.g. CdTe or CZT):

- spatial resolution (<mm) achieved with ~ 10 times larger photodetector pixel size
 $\Rightarrow 1/100$ readout channels needed for a given spatial resolution
- good detection efficiency, adjustable vs. energy with scintillator thickness

Main disadvantage

Poorer energy resolution, especially at low energy, due to the scintillator conversion (although new scintillators like LaBr_3 are reducing this gap) and to the electronics noise added by the several photodetectors used for the light readout

Small prototype of SDD - CsI(Tl) Anger camera



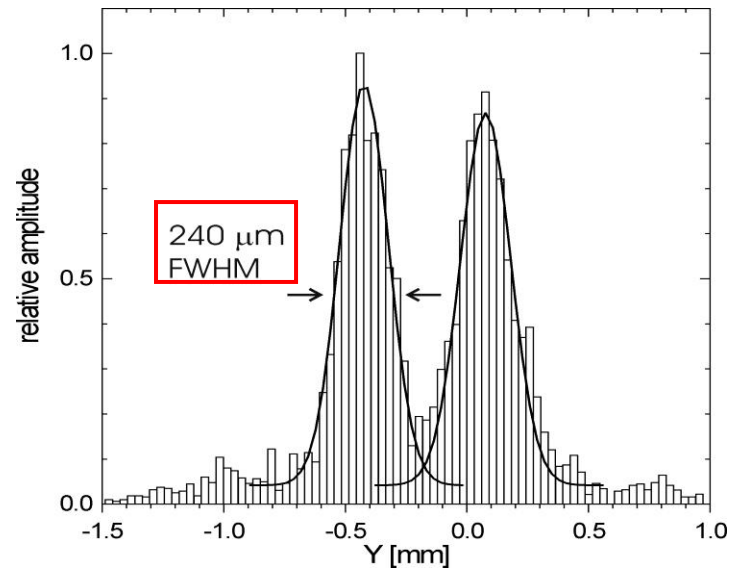
Total area = $5 \text{ mm}^2 \times 19 \sim 1 \text{ cm}^2$

CsI(Tl) thickness = 3 mm

$T = -10^\circ\text{C}$

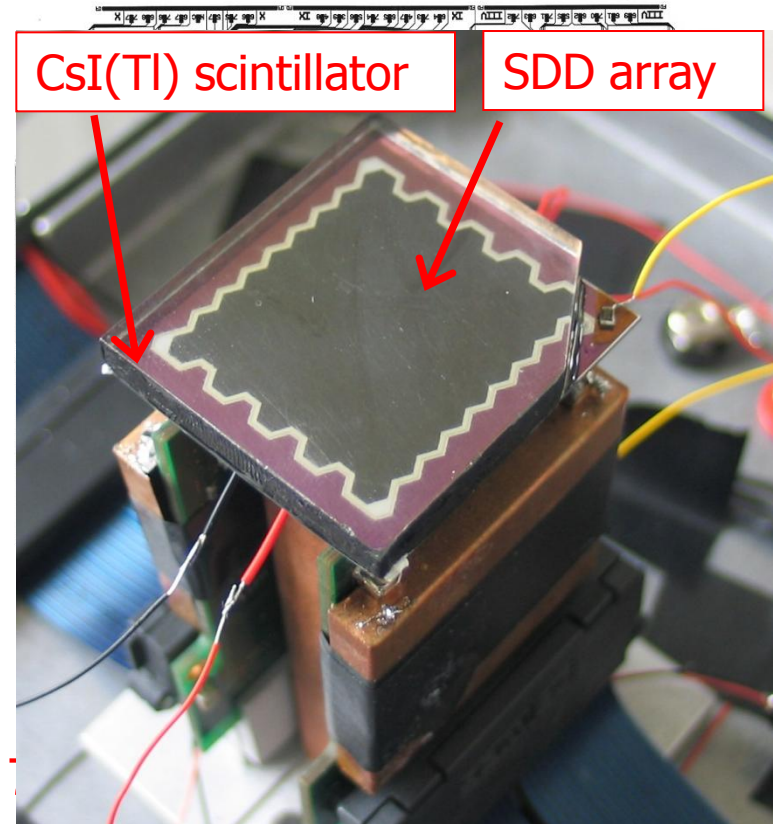
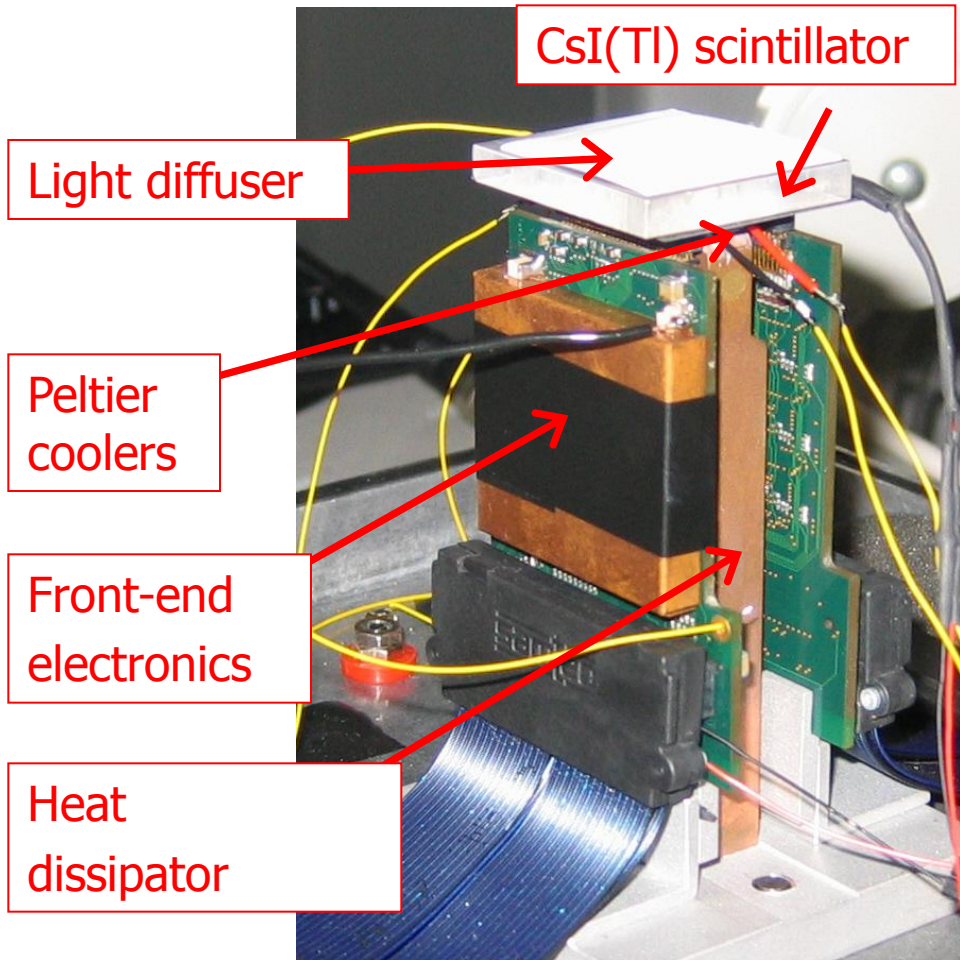
$E = 122 \text{ keV}$ (^{57}Co)

\varnothing collimator $\sim 180 \mu\text{m}$



160 μm
intrinsic
resolution

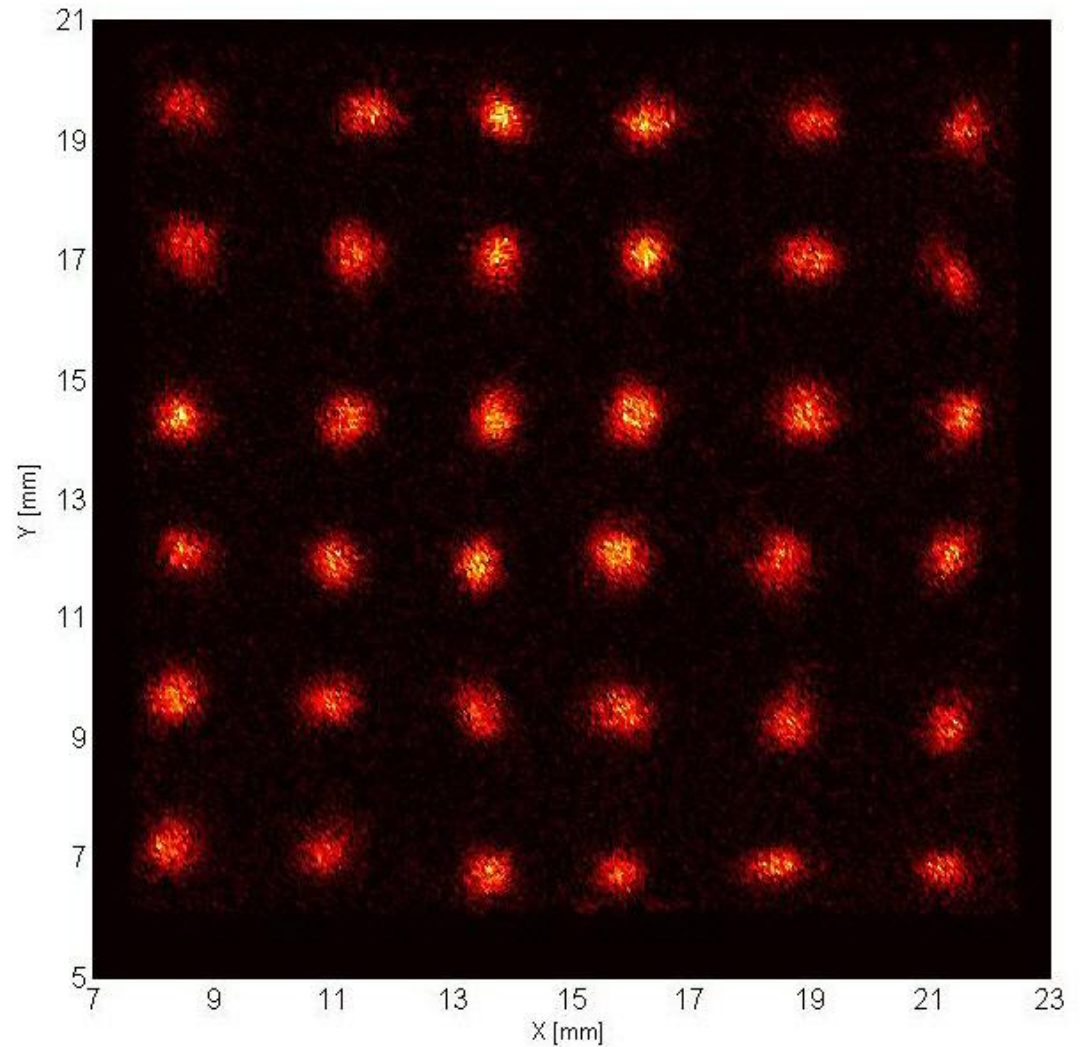
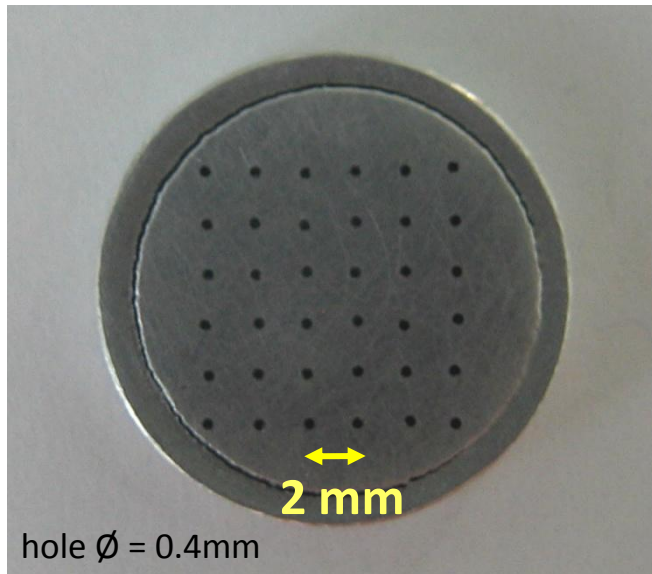
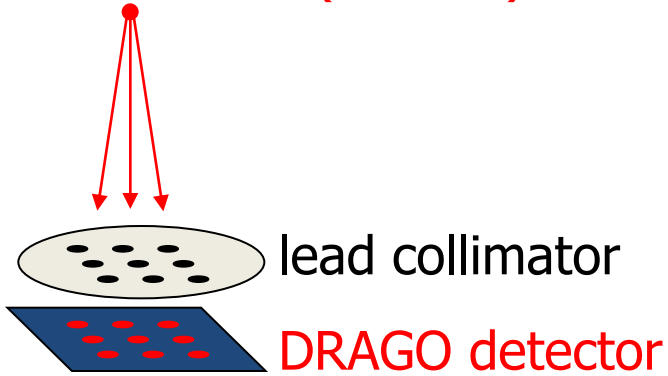
The DRAGO Gamma Camera (DRift detector Array-based Gamma camera for Oncology)



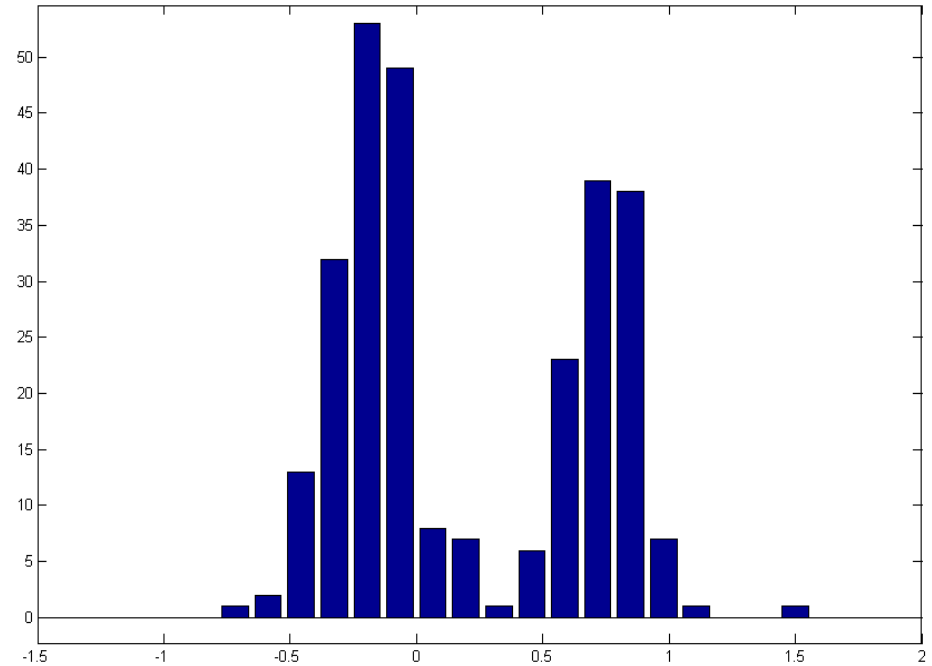
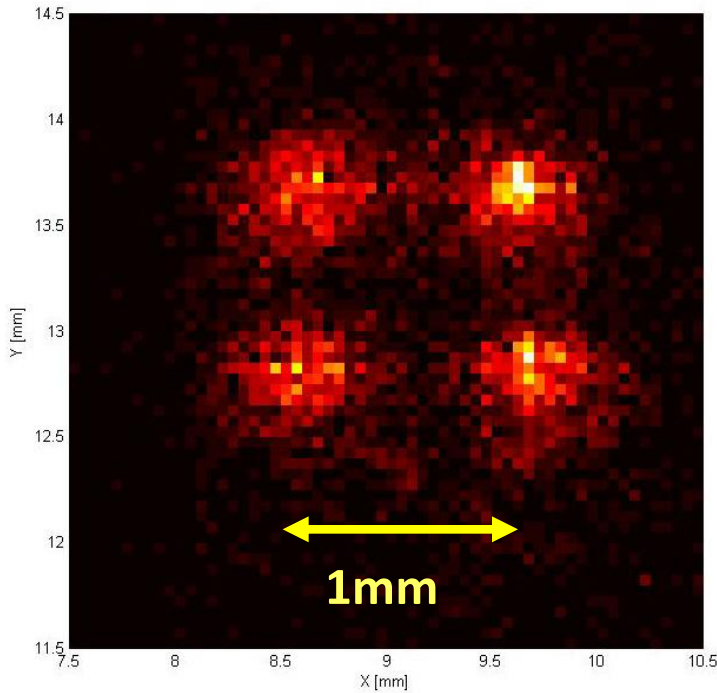
- tot. active area = 6.7 cm^2
- CsI(Tl) thickness = 5 mm
- leakage current = 300 pA/cm^2 @ RT
- $\epsilon = 80\%$ @ 140 keV
- QE = 90% @ 565 nm of CsI(Tl)

γ -ray measurements

^{57}Co source (122keV)



Spatial resolution

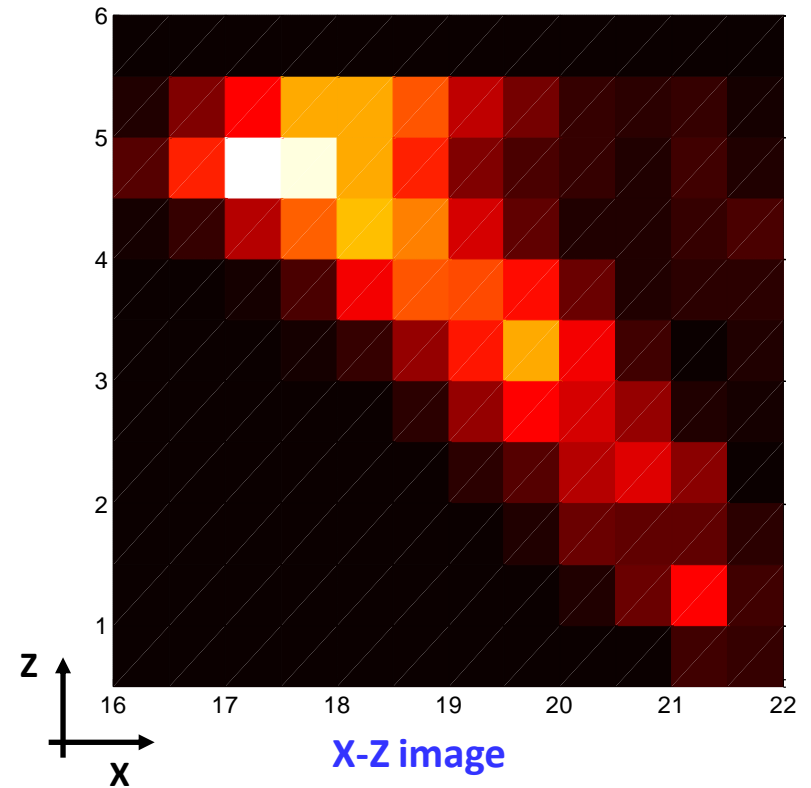
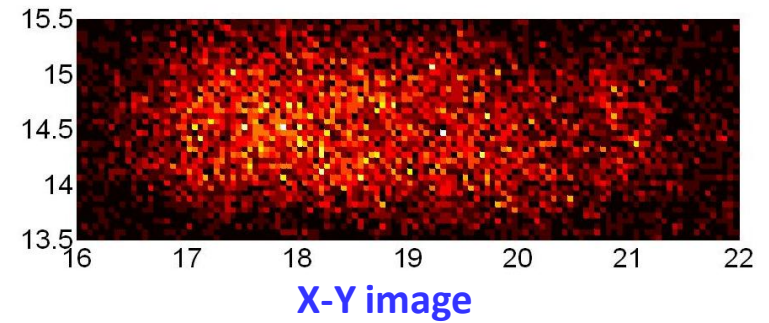
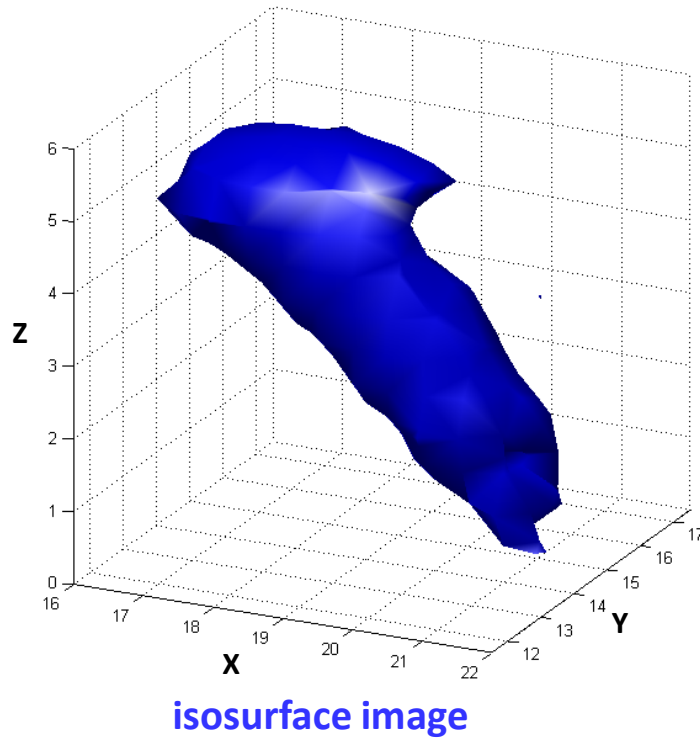
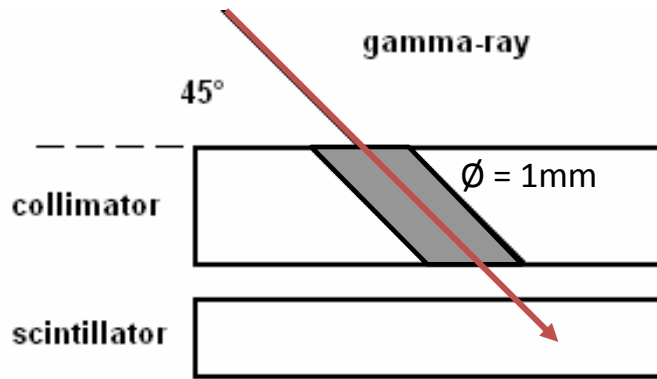


\emptyset collimator \sim 0.2 mm

Spatial resolution = 0.25 – 0.50 mm

(ref: 3.2mm SDD pixel size)

Verification of DOI capability by measuring a 45° tilted beam



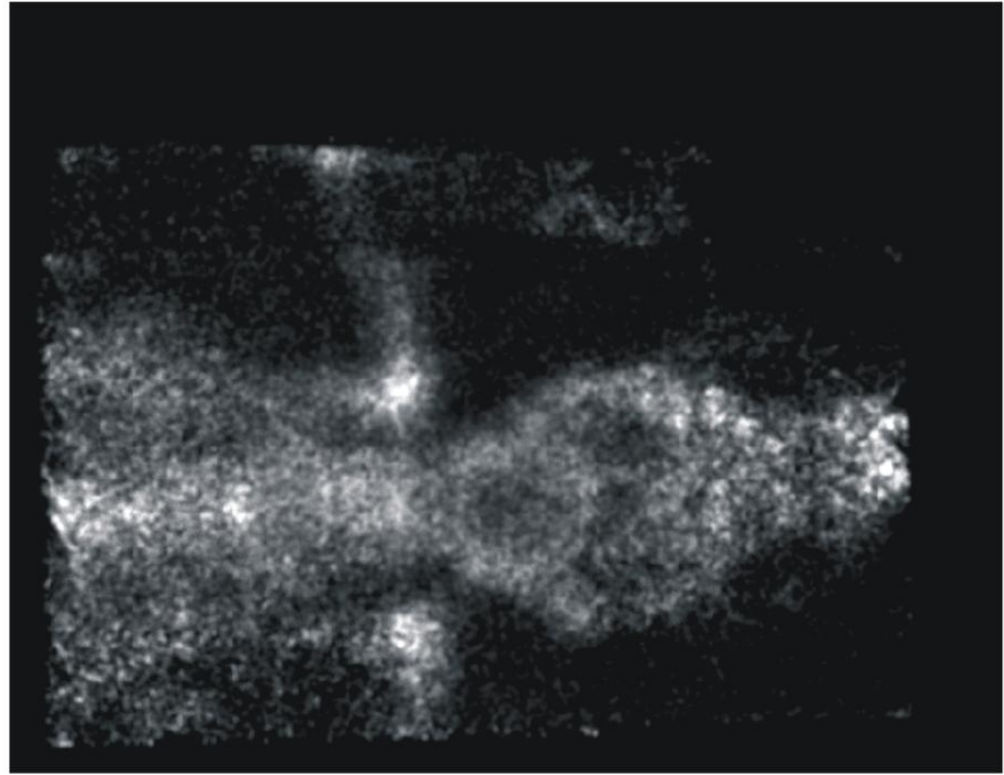
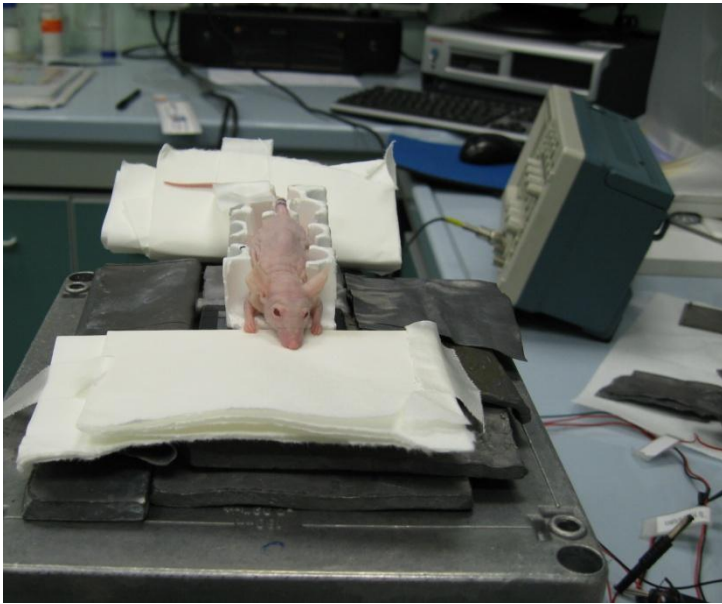
Preliminar *in vivo* planar scintigraphy of a mouse

[⁹⁹Tc] MDP

2.5mCi injected activity

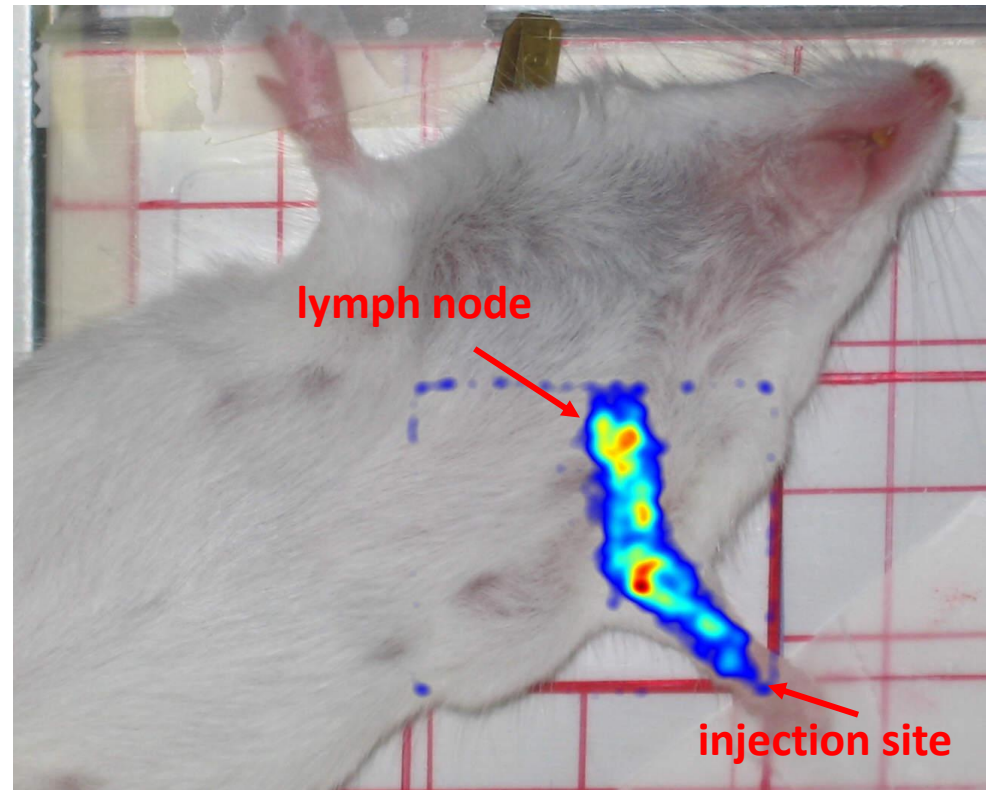
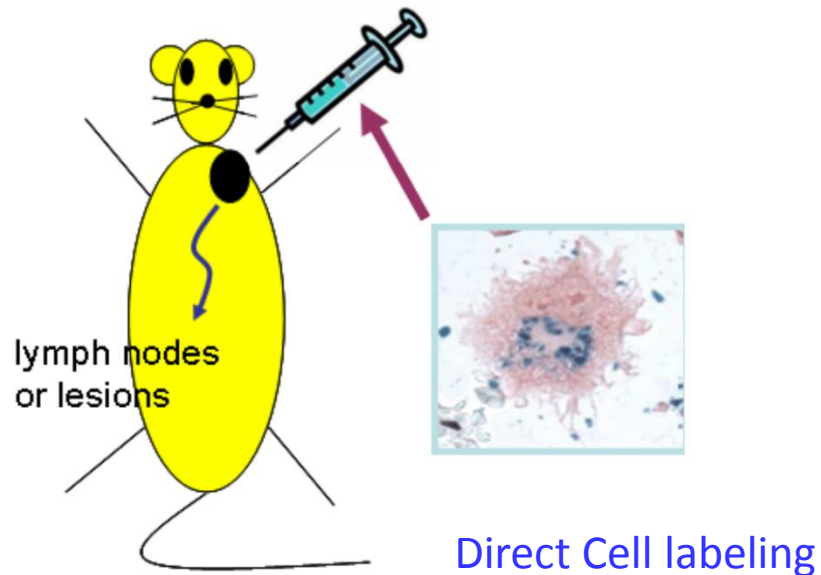
2h. after injection,

10min acquisition time



Measurements carried out at
Hospital San Raffaele, Milano, Italy
Hospital San Paolo, Milano, Italy

Preliminar *in vivo*
Direct Cell imaging



In-vivo dendritic cells tracking by means of the DRAGO camera

Measurements carried out at
Hospital San Paolo, Milano, Italy



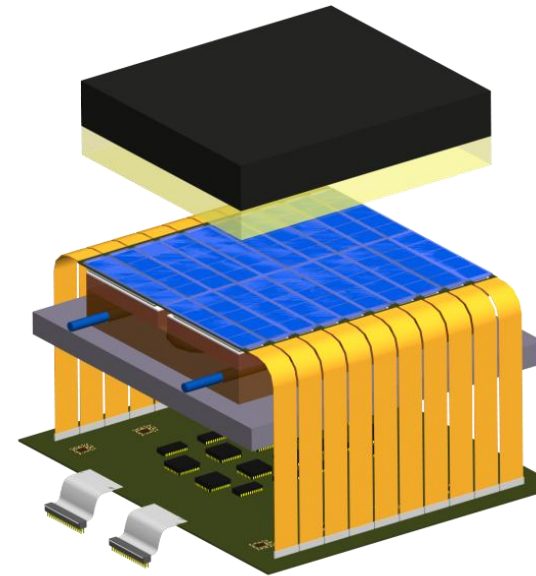
The HICAM gamma camera (EC contract n. LSHC-CT-2006-037737)

features:

- **10x10cm²** FOV
- intrinsic resolution ~ **1mm**
- overall resolution ~ 2.5mm @5cm
- energy resolution ~ 10% @140keV
- **compactness**
- compatibility with MRI

Applications:

- planar clinical studies of spine and small bones
- intra-operative imaging of breast cancer and melanoma
- imaging of parathyroid and thyroid
- SPECT measures in test phantoms
- combined HI-CAM and MRI measures
- small animal imaging

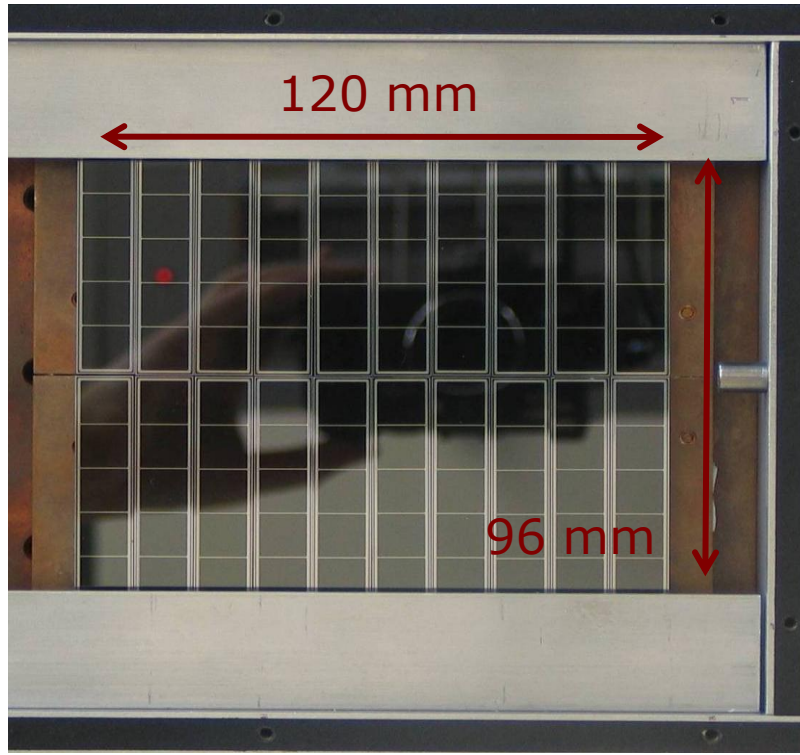


The consortium:

- Politecnico di Milano, Italy
- MPI Halbleiterlabor, Germany
- L'ACN, Italy
- Nuclear Fields Holland
- UCL London, UK
- OORR-Bg, Italy
- Hospital San Pau, Barcelona, Spain
- University of Milan, Italy
- Cf Consulting, Italy

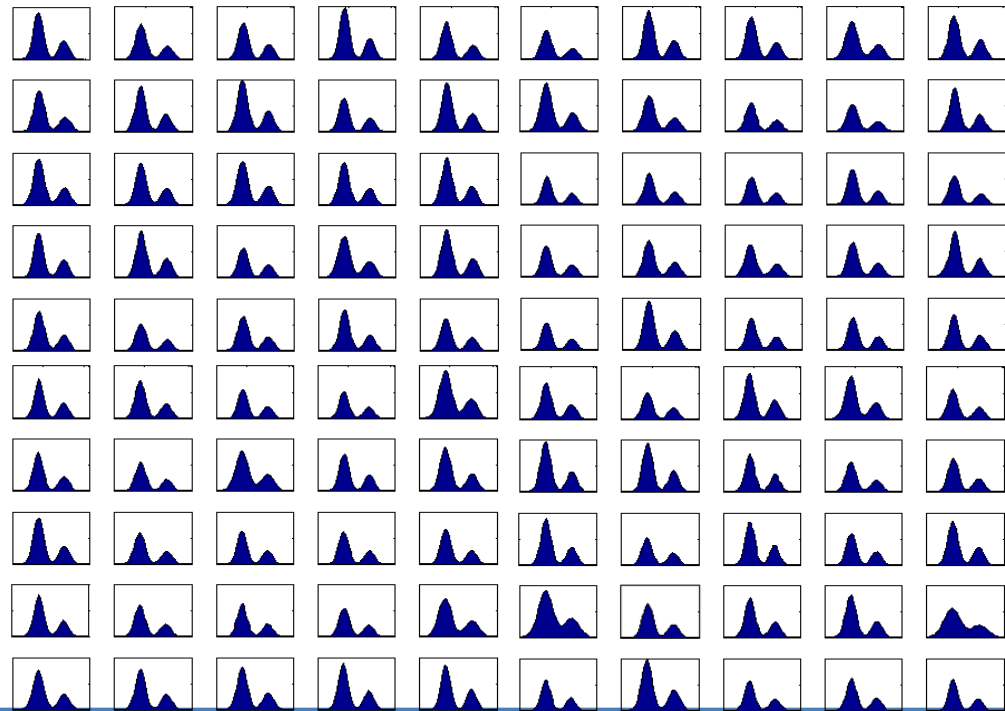


Array of 20 monolithic arrays of 5 SDDs (100cm² total area)



The biggest array of assembled SDDs

Photodetectors qualification:
direct ⁵⁵Fe irradiation
(without the scintillator)



~ 20% dead area

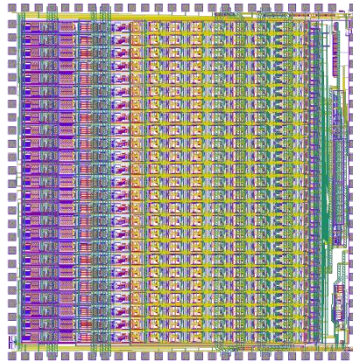
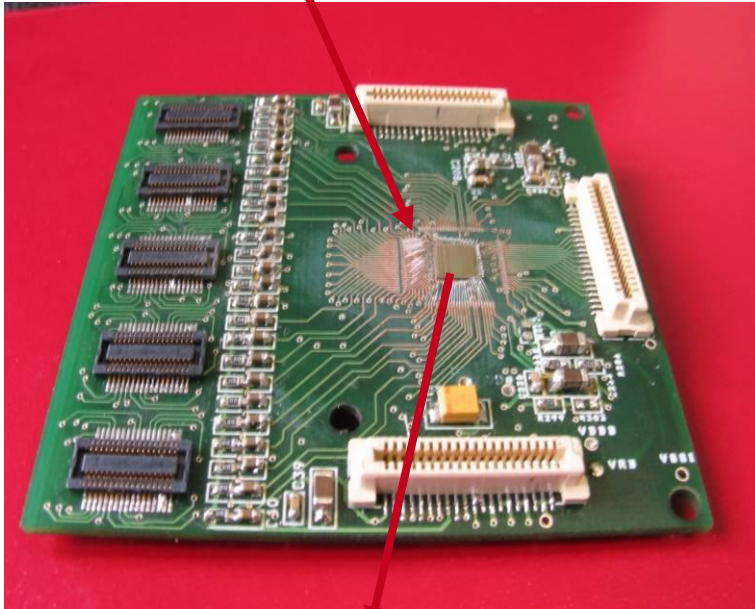
$$t_{\text{peak}} = 8.3 \mu\text{s}$$

$$T = -5^\circ\text{C}$$



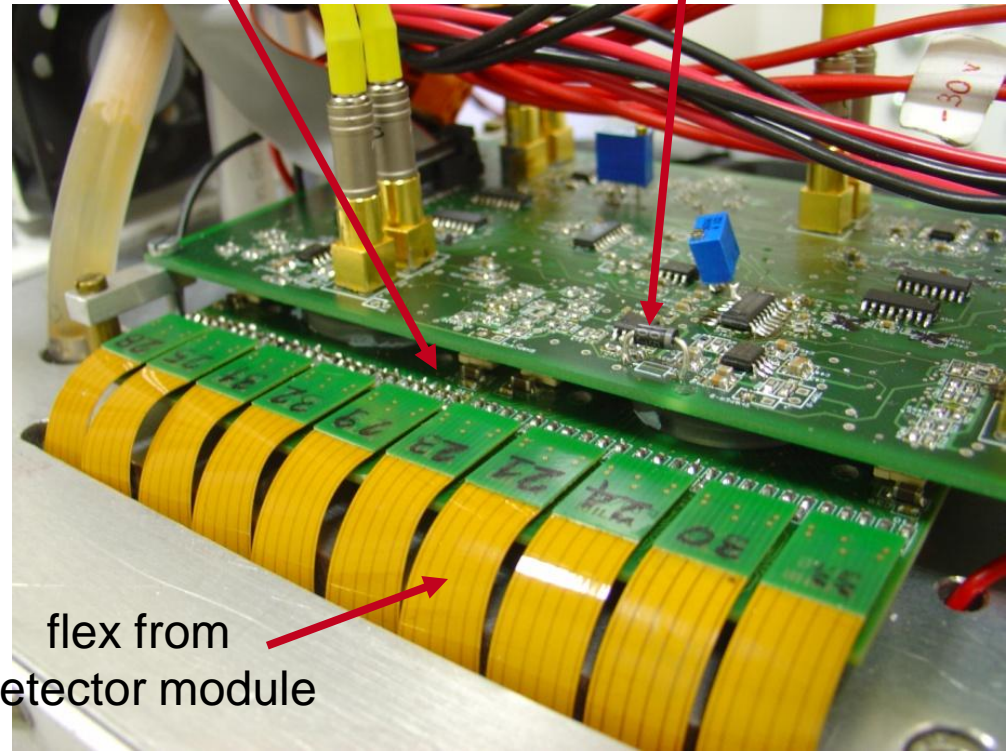
Biassing and readout electronics of the camera

25-channels readout circuit
0.35 μm CMOS technology



25-channels
readout boards
(x4)

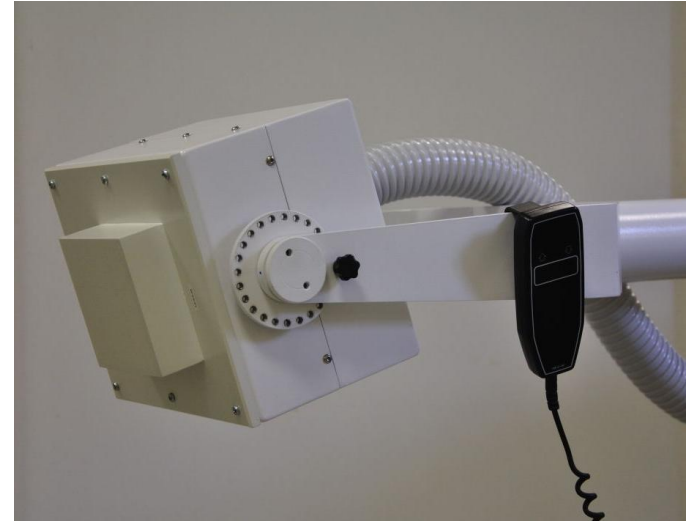
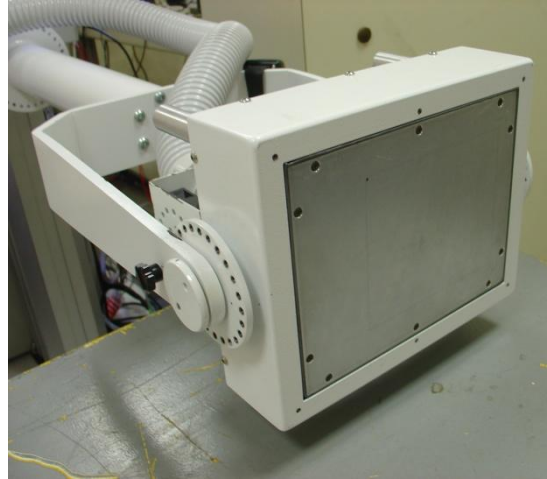
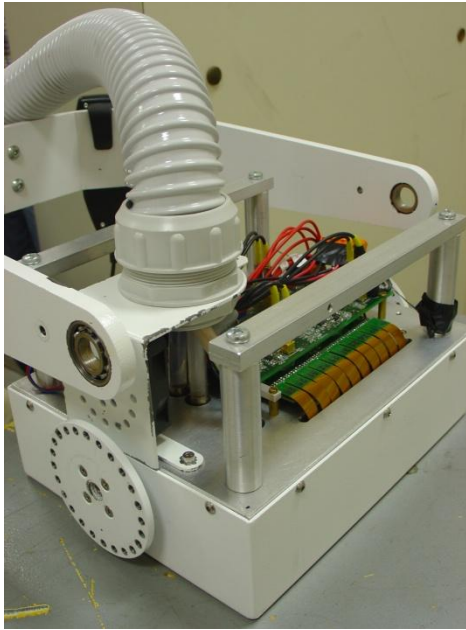
board including biasing
and interface with DAQ
(SPI programming and
data acquisition)



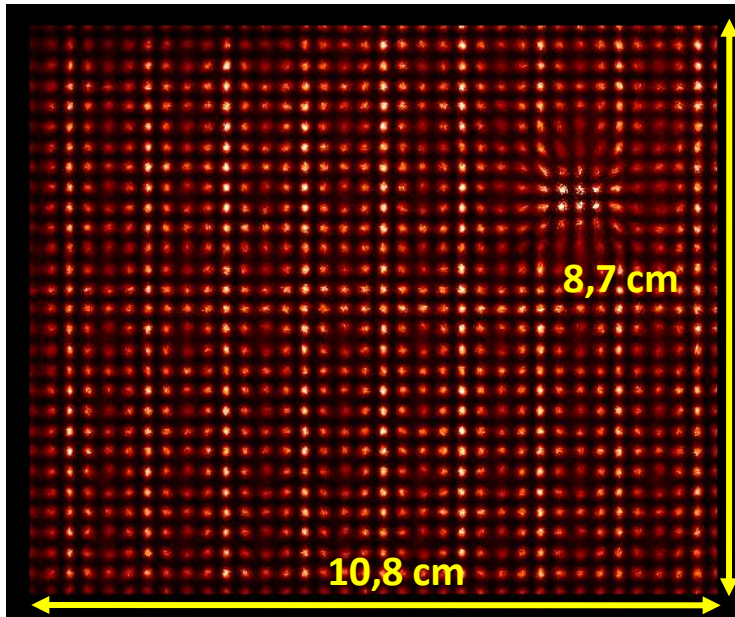
flex from
detector module



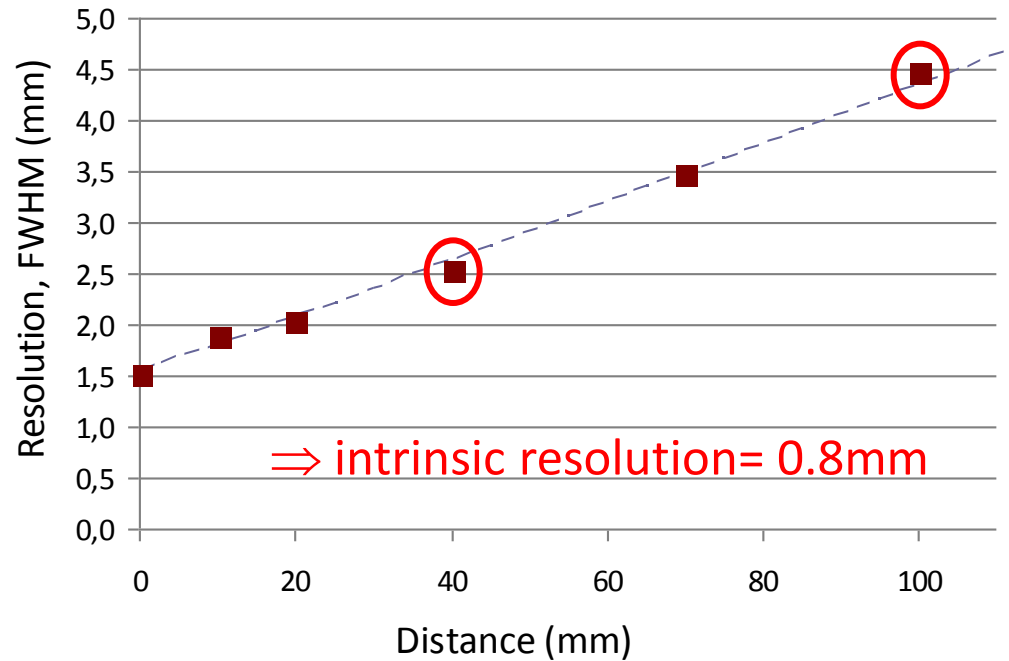
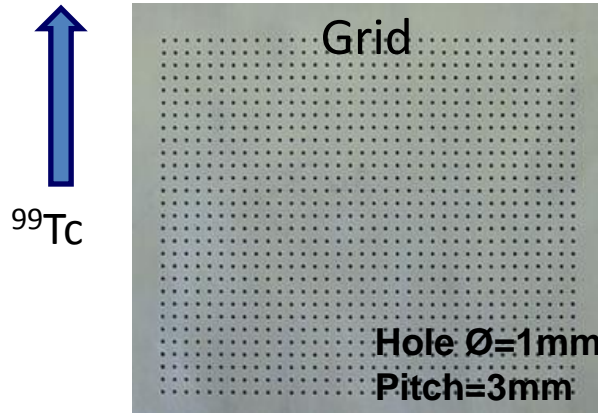
Assembly of the camera head



FOV and spatial resolution



corrected for linearity and uniformity



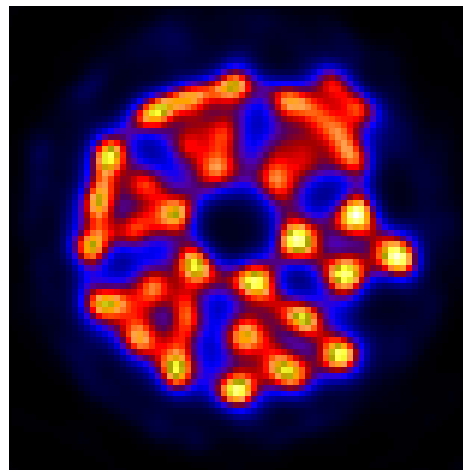
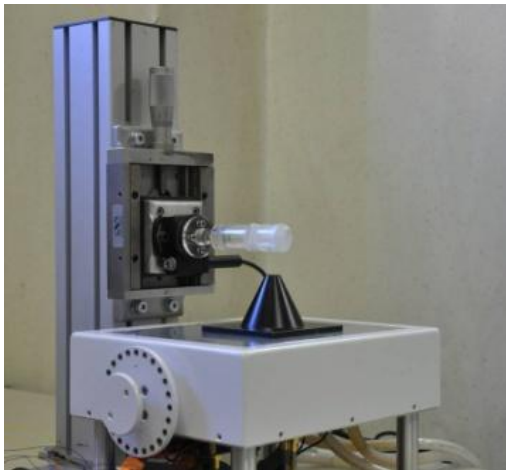
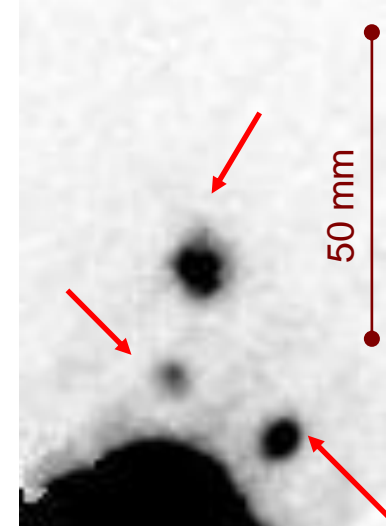
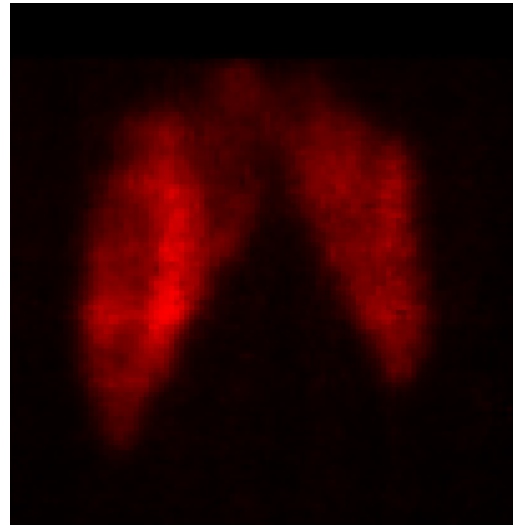
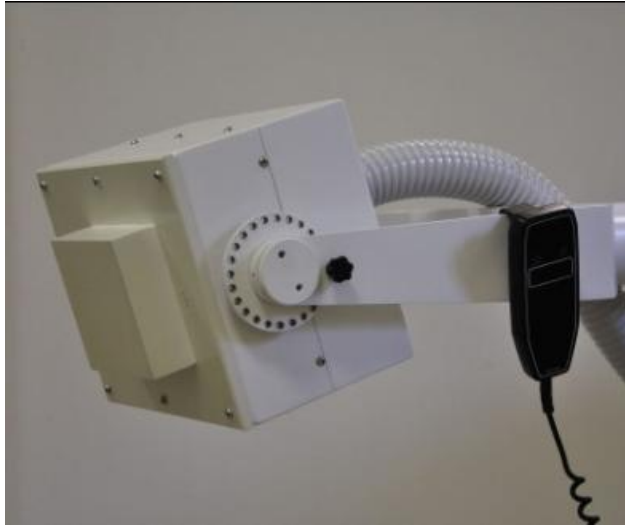
LEUHR parallel hole collimator

Comparison with a reference camera

E.CAM System Spatial Resolution:

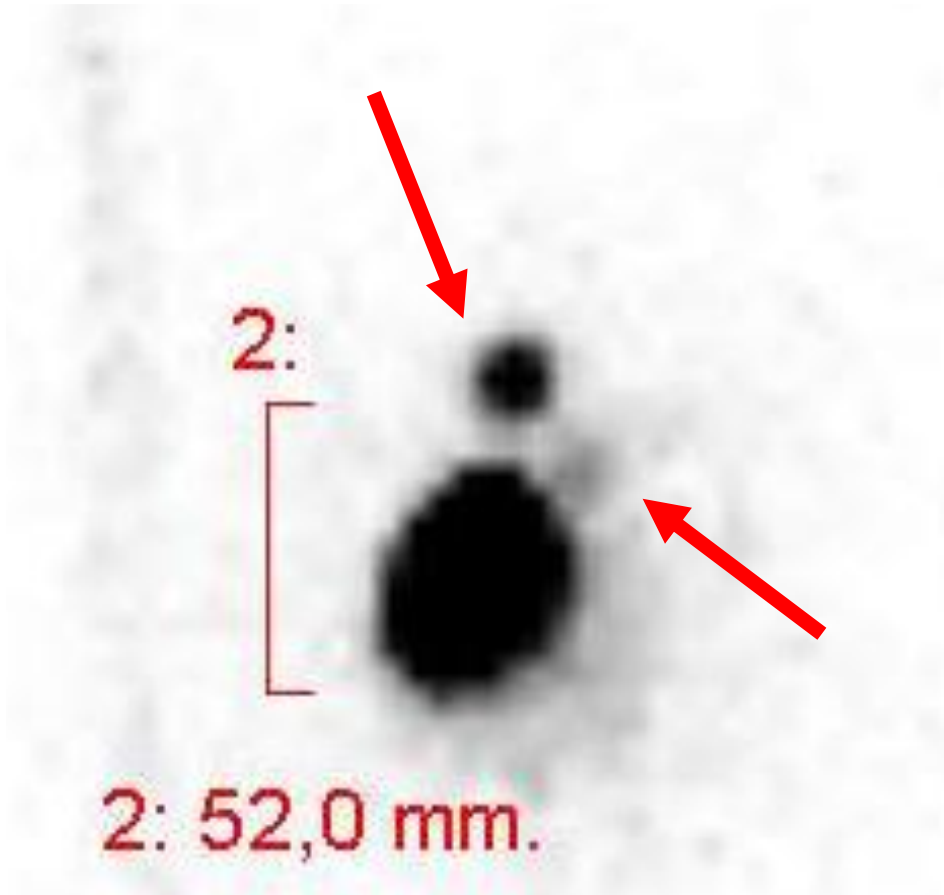
6.3 mm with LEUHR @ 10 cm

Applications of the HICAM gamma camera

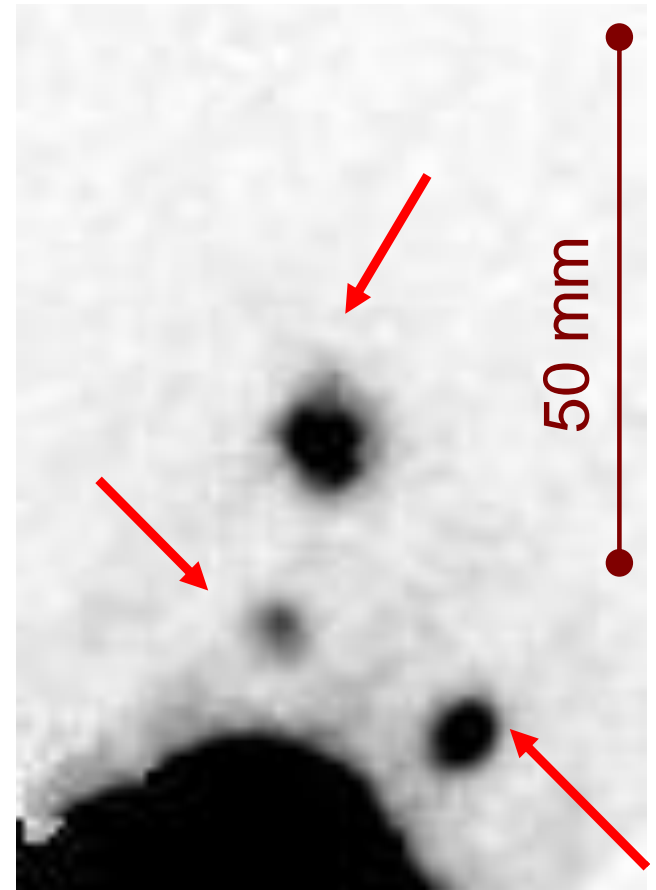


Clinical trial: Lymphoscintigraphy

Lymphoscintigraphy to localize the sentinel node



E-CAM

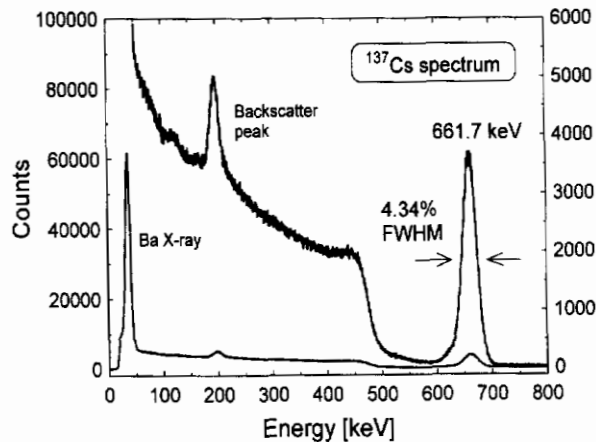


HICAM

Summary: 15 years of research and development

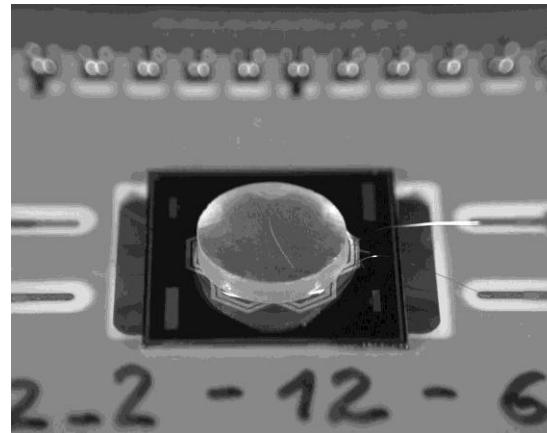
1997

First SDD-scintillator
gamma detector
world-record energy
resolution
(0.07cm²)



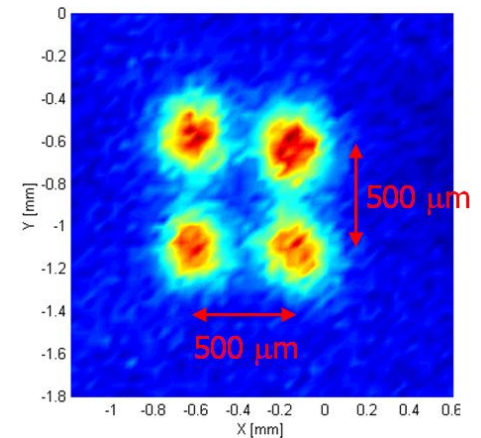
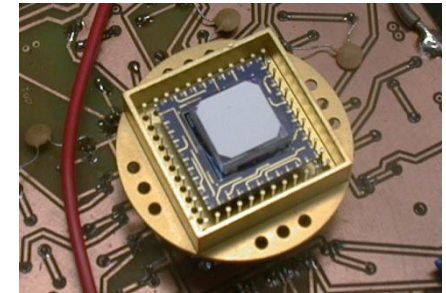
2000

proof of a SDD-
based gamma-ray
imaging detector
(0.35cm²)



2004

200μm resolution
gamma camera
(1cm²)

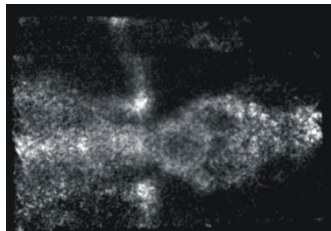
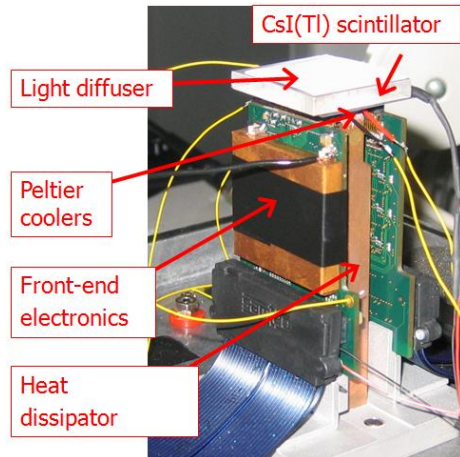


2007

The DRAGO gamma camera

first animal imaging

(7cm²)

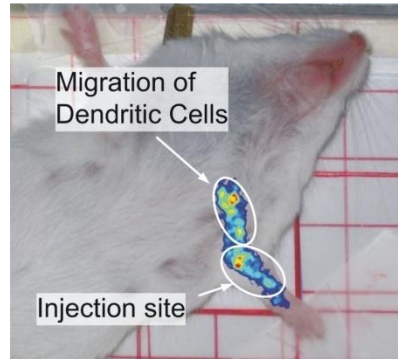
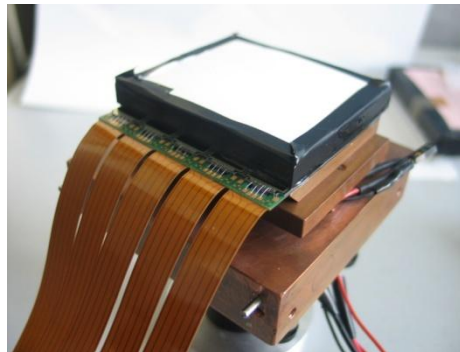


2009

The HICAM gamma camera

first cellular imaging

(25cm²)



2010

The large HICAM gamma camera

first clinical imaging

(100cm²)

